

International Journal of Cardiovascular Imaging

Altered coronary endothelial function in young smokers detected by magnetic resonance assessment of myocardial blood flow during the cold pressor test --Manuscript Draft--

Manuscript Number:	CAIM-D-13-00592R1
Full Title:	Altered coronary endothelial function in young smokers detected by magnetic resonance assessment of myocardial blood flow during the cold pressor test
Article Type:	ASCI Special Issue
Keywords:	Coronary endothelial function; myocardial blood flow; cold pressor test; Magnetic resonance imaging; smoking
Corresponding Author:	YASUTAKA ICHIKAWA, M.D. Mie University Hospital Tsu, Mie JAPAN
Corresponding Author Secondary Information:	
Corresponding Author's Institution:	Mie University Hospital
Corresponding Author's Secondary Institution:	
First Author:	YASUTAKA ICHIKAWA, M.D.
First Author Secondary Information:	
Order of Authors:	YASUTAKA ICHIKAWA, M.D. KAKUYA KITAGAWA, M.D. SHINGO KATO, M.D. KAORU DOHI, M.D. TADANORI HIRANO, M.D. MASAAKI ITO, M.D. HAJIME SAKUMA, M.D.
Order of Authors Secondary Information:	
Abstract:	<p>Endothelial dysfunction is a key element in early atherogenesis. The purposes of this study were to evaluate the feasibility of magnetic resonance (MR) assessment of altered myocardial blood flow (MBF) in response to the cold pressor test (CPT), and to determine if coronary endothelial dysfunction in young smokers can be detected with this noninvasive approach. Fourteen healthy non-smokers (31 ± 6 years) and 12 smokers (34 ± 8 years) were studied. Breath-hold phase-contrast cine MR imaging (PC-MRI) of the coronary sinus (CS) were obtained at rest and during the CPT. MBF was measured as CS flow divided by LV mass and the rate pressure product. In non-smokers, MBF was 0.88 ± 0.19 ml/min/g at rest and significantly increased to 1.13 ± 0.26 ml/min/g during the CPT ($P = 0.0001$). In smokers, MBF was 0.94 ± 0.26 ml/min/g at rest and 0.96 ± 0.30 ml/min/g during the CPT ($P = 0.73$). ΔMBF (MBF during the CPT - MBF at rest) was significantly reduced in smokers compared with non-smokers (0.02 ± 0.20 ml/min/g vs. 0.26 ± 0.18 ml/min/g, $P = 0.005$). The intra-class correlation coefficient between measurements by two observers was 0.90 for ΔMBF. A significant reduction in MBF response to CPT was demonstrated in young smokers with PC-MRI at 1.5 tesla. This noninvasive method has great potential for assessment of coronary endothelial function.</p>
Response to Reviewers:	Dear T-H Kim, Guest Editor We thank you for giving us an opportunity for publication of International Journal of Cardiovascular Imaging.

As the reviewer suggested, we revised the final paragraph in the introduction section.
The revision has been uploaded.

We wish to express in advance our great appreciation for the time and consideration of
the reviewers and editors regarding our revised manuscript.

Sincerely,

Yasutaka Ichikawa, M.D.
Department of Radiology, Mie University Hospital
E-mail: yasutaka@clin.medic.mie-u.ac.jp

Original research paper

Altered coronary endothelial function in young smokers detected by magnetic resonance assessment of myocardial blood flow during the cold pressor test

Yasutaka Ichikawa, MD¹, Kakuya Kitagawa, MD², Shingo Kato, MD²,
Kaoru Dohi, MD³, Tadanori Hirano, MD¹, Masaaki Ito, MD³, Hajime Sakuma, MD²

¹Department of Radiology, Matsusaka Central Hospital, 102 Kobou, Kawai,
Matsusaka, Mie, 515-8566 Japan

²Department of Radiology, and ³Department of Cardiology, Mie University Hospital,
2-174 Edobashi, Tsu, Mie 514-8507, Japan

The authors report no conflicts of interest.

Total word account: 4626 words

Three tables and 6 figures

Brief title: Coronary sinus flow during the cold pressor test

Address for correspondence: Yasutaka Ichikawa, MD
Department of Radiology, Matsusaka Central Hospital
102 Kobou, Kawai, Matsusaka, Mie 515-8566, Japan
Phone: +81-598-21-5252 ; Fax: +81-59-232-8066
E-mail: yasutaka@clin.medic.mie-u.ac.jp

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43 **Keywords** Coronary endothelial function · Myocardial blood flow · Cold pressor
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45 test · Magnetic resonance imaging · Smoking
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Introduction

The endothelium plays an important role in antiatherosclerotic and antithrombotic events in vessels [1-2]. Patients with coronary endothelial dysfunction have a higher cardiovascular event rate than those with normal coronary vasomotion [3-4]. Several mechanisms contribute to impairment of endothelial function [5-6]; for example, chronic smoking may cause endothelial dysfunction in subjects without epicardial coronary artery stenosis [7-9].

The cold pressor test (CPT) has been used as one of several approaches to evaluate endothelial function [10-13]. In healthy subjects, the vasodilatory effect of the CPT is mediated through a central sympathetic response which stimulates the release of nitric oxide from the coronary endothelium [11]. Prior studies have shown that a vasoconstrictive response to the CPT is observed in angiographically normal subjects with cardiovascular risk factors [14-15], and that such a response is an independent predictor of future cardiac events [15]. Thus, a flow response to CPT might be a sensitive measure of coronary endothelial dysfunction in the early stages of atherosclerosis.

Phase-contrast cine magnetic resonance imaging (PC-MRI) of coronary sinus (CS) blood flow can provide a noninvasive estimate of total myocardial blood flow (MBF) [16], because the CS drains over 96% of the myocardial venous blood from the left ventricle (LV) [17]. Quantification of CS flow using PC-MRI in response to vasodilator pharmacological stress has been used to assess coronary flow reserve in patients with hypertrophic cardiomyopathy, heart failure and dilated cardiomyopathy [18-20]. In a more recent study by Maroules et al. [21], they investigated coronary flow response to CPT in asymptomatic women using spiral velocity encoded MRI at 3

1 tesla. However, the spiral velocity encoded sequence at 3 tesla is a research pulse
2 sequence that is not available in clinical cardiac MRI studies. In addition, altered MBF
3 response to CPT in subjects with abnormal endothelial function compared with
4 control subjects due to smoking or atherosclerosis has not been investigated.
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10 The purposes of this study were to evaluate the feasibility and intra- and
11 inter-observer variabilities of measuring MBF alteration during the CPT by using a 1.5
12 tesla MR system and a PC-MRI sequence that are widely available, and to determine
13 if impaired coronary endothelial dysfunction in smokers can be detected with this
14 noninvasive approach.
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24 **Methods**

25 **Study population**

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29 The study population consisted of 14 healthy male non-smokers (mean age, $30.9 \pm$
30 5.9 years) and 12 healthy male smokers (mean age, 33.8 ± 7.8 years) who had been
31 smoking ≥ 5 years (range, 5–20 years) and a total of 10.6 ± 8.0 pack-years (1
32 pack-year is defined as smoking of 20 cigarettes per day for 1 year or the equivalent).
33
34 All subjects were male and non-obese (body mass index < 27 kg/m²), and did not
35 have hypertension, diabetes or a family history of vascular disease. They were
36 clinically well and taking no regular cardiovascular medication or antioxidant vitamin
37 supplementation. Before MRI examination, all subjects abstained from consuming
38 caffeine and alcohol and from smoking for at least 12 hours, and from consuming
39 flavonoid-containing food for at least 24 hours. This study was approved by the local
40 Institutional Review Board, and all participants provided written informed consent.
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3 MRI acquisition
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7 MRI was acquired at 1.5 tesla with 5-channel cardiac coils (Achieva, Nova-dual
8 gradient; Philips Medical Systems, Best, The Netherlands). After placement of
9 vector-electrocardiographic monitoring leads, subjects underwent imaging in the
10 supine position. For cardiac orientation, scout images were acquired in three
11 orthogonal planes. After acquiring vertical long axis and horizontal long axis cine
12 images of the LV using a steady-state free precession sequence, short-axis cine
13 images of the LV were acquired from apex to base with suspended shallow
14 breath-holds (repetition time = 3.2 ms, echo time = 1.6 ms, flip angle = 55°, field of
15 view = 350 × 350 mm, reconstruction matrix = 256 × 256, reconstruction pixel size =
16 1.37 × 1.37 mm, slice thickness = 10 mm, and phases per cardiac cycle = 20).
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31 To identify the location of the CS, axial plane breath-hold cine MRI was
32 obtained through the atrioventricular groove (repetition time = 2.9 ms, echo time = 1.5
33 ms, flip angle = 55°, field of view = 350 × 350 mm, reconstruction matrix = 256 × 256,
34 reconstruction pixel size = 1.37 × 1.37 mm, slice thickness = 5 mm, and phases per
35 cardiac cycle = 20) (Fig. 1). The imaging plane for PC-MRI was placed perpendicular
36 to the CS, approximately 1 to 2 cm proximal to the entrance of the CS into the right
37 atrium and distal to the merging portion of the middle cardiac vein. CS flow
38 measurements were obtained during a suspended shallow breath-hold using an
39 electrocardiography-triggered turbo phase contrast field echo sequence with k-space
40 segmentation (repetition time = 5.6 ms, echo time = 3.6 ms, flip angle = 15°, slice
41 thickness = 5 mm, field of view = 240 × 194 mm, acquisition matrix = 160 × 112,
42 acquisition pixel size = 1.5 × 1.7 mm, velocity encoding = ± 50 cm/s, reconstruction
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1 matrix = 256×256 , reconstruction resolution = 0.9×0.9 mm, and phases per cardiac
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3 cycle = 20).
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6 7 Cold pressor test 8 9

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11 After acquisition of cine MRI of the LV and PC-MRI of the CS at rest, the subject's foot
12 was immersed in a MRI-compatible ice-water bath (at a temperature of approximately
13 7°C) for 2 minutes. After 1 minute of foot immersion, flow measurement of the CS was
14 performed during the CPT. Heart rate and blood pressure were measured using a
15 noninvasive and MRI-compatible electrocardiogram and calf blood pressure monitor
16 at baseline and at 30-s intervals throughout each study. The rate-pressure product
17 (RPP) was calculated as systolic blood pressure \times heart rate.
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31 Image analysis 32 33 34 35

36 Cine MRI and PC-MRI were analyzed using a workstation (ViewForum, Philips
37 Medical Systems, Best, The Netherlands). For measurement of LV mass and LV
38 volume, two independent observers manually traced epi- and endo-cardial borders of
39 the LV wall on short axis cine images at end-diastole and end-systole. LV mass was
40 calculated as the sum of myocardial areas multiplied by the slice thickness and the
41 density (1.05 g/ml) of myocardial tissue [22].
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50 CS flow was measured by tracing the CS contour on each magnitude image
51 throughout the cardiac cycle by two independent observers blinded to both subject
52 group (control vs. smoker) and state (rest vs. CPT). The area of the CS was recorded,
53 and the traced region was automatically transferred to the corresponding phase
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1 images in order to measure average flow velocity in the CS. Phasic blood flow was
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3 calculated as the product of the area and spatial average flow velocity. Mean volume
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5 flow was derived by means of integration of phasic flow over time. To compensate for
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7 the through-plane motion and phase offset error, a second region of interest was
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9 traced for each phase image on the adjacent tissue of CS [18, 23]. Flow velocity in
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11 each pixel within the vessel lumen was corrected by subtracting the mean velocity in
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13 the second region of interest. According to previous studies [23-25], MBF (ml/min/g)
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15 was calculated as follows: $MBF = (CS \text{ flow} / (RPP \times LV \text{ mass})) \times 7500$. The difference
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17 between MBF during the CPT and at rest and the percent change of MBF during the
18
19 CPT were calculated as follows:
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22 $\Delta MBF = MBF \text{ during the CPT} - MBF \text{ at rest}$, and
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24 $\text{Percent change of MBF (\%)} = \Delta MBF / MBF \text{ at rest} \times 100$.
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31 Statistical analysis 32 33 34 35

36 Data were statistically analyzed using SPSS software, version 11.5 (SPSS, Inc.,
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38 Chicago, IL, USA). Continuous values are presented as mean \pm standard deviation or
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40 as median and interquartile range (IQR). MRI data are reported as an average of
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42 measurements recorded by two observers. Differences between control subjects and
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44 smokers in age, height, weight, BMI, LV end-diastolic volume, ejection fraction, LV
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46 mass, MBF, ΔMBF , and percent change of MBF were tested with the unpaired
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48 Student's *t*-test. Differences in LV end-systolic volume between control subjects and
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50 smokers were analyzed by the Mann-Whitney *U* test. The effect of the CPT on blood
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52 pressure, heart rate, and MBF was analyzed by the paired Student's *t*-test. For
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54 investigating the effect of the CPT on RPP, the Wilcoxon signed-rank test was used.
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1 For correlation analysis, we calculated Spearman's correlation coefficients. Inter- and
2 intra-observer variabilities in measuring MBF and Δ MBF were evaluated using an
3 intra-class correlation coefficient (ICC), the Bland-Altman method [26] and a
4 repeatability coefficient. The repeatability coefficient was calculated as 1.96 times the
5 standard deviation of the differences, as proposed by Bland and Altman [26]. All *P*
6 values < 0.05 were considered to represent statistical significance.
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17 Results

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22 Clinical characteristics of all 26 subjects are shown in Table 1. There were no
23 significant differences in clinical characteristics between smokers and non-smokers.
24 No significant differences were found between non-smokers and smokers for LV
25 end-diastolic volume, end-systolic volume, ejection fraction, heart rate or LV mass
26 (159.6 \pm 14.4 ml vs. 163.8 \pm 24.2 ml, *P* = 0.60; 62.2 \pm 7.6 ml vs. 62.4 \pm 13.9 ml, *P* =
27 0.96; 63.1 \pm 7.6% vs. 62.1 \pm 4.2%, *P* = 0.68; 61.9 \pm 9.3 beats/min vs. 63.5 \pm 9.9
28 beats/min, *P* = 0.67; and 88.1 \pm 9.4 g vs. 90.4 \pm 11.6 g, *P* = 0.58, respectively).
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39 PC-MRI was acquired at rest and during the CPT at diagnostic quality in all
40 subjects. Representative CS volume flow curves in the cardiac cycle are shown in
41 Figure 2. Peak volume flow in the CS was observed during early diastole.
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45 Hemodynamic parameters and MBF values at rest and during the CPT are shown in
46 Table 2.
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51 In non-smokers, MBF was 0.88 \pm 0.19 ml/min/g at rest, and significantly
52 increased to 1.13 \pm 0.26 ml/min/g during the CPT (*P* = 0.0001). In smokers, MBF was
53 0.94 \pm 0.26 ml/min/g at rest and 0.96 \pm 0.30 ml/min/g during the CPT (*P* = 0.73).
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57 Individual Δ MBF values and percent change of MBF are shown in Figure 3. Mean
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1 Δ MBF during the CPT in smokers (0.02 ± 0.20 ml/min/g [95% CI: 0.16 to 0.35
2 ml/min/g]) was significantly lower than in non-smokers (0.26 ± 0.18 ml/min/g [95% CI:
3 -0.10 to 0.14 ml/min/g], $P = 0.005$). The mean percent change of MBF in smokers
4 was also significantly lower than in non-smokers ($3.6 \pm 19.7\%$ vs. $30.7 \pm 21.3\%$, $P =$
5 0.003). There was no significant correlation between pack-years and percent change
6 of MBF in smokers ($r = -0.39$, $P = 0.20$) (Fig. 4).
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14 Inter- and intra-observer variation in MBF measurements are summarized in
15 Table 3. The ICC between the measurements by the two observers was 0.91 for MBF
16 at rest, 0.96 for MBF during the CPT and 0.90 for Δ MBF. Bland-Altman plots of inter-
17 and intra-observer variabilities in measuring Δ MBF and percent change of MBF are
18 presented in Figures 5 and 6, respectively. The mean difference between the two
19 observers was 0.03 ± 0.10 ml/min/g for Δ MBF and $2.3 \pm 12.7\%$ for percent change of
20 MBF.
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34 Discussion

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39 The present study demonstrated that noninvasive assessment of MBF response to
40 CPT using PC-MRI can provide detection of altered endothelial function in coronary
41 circulation. Impaired coronary endothelial function in healthy smokers was detected
42 with PC-MRI at 1.5 tesla without administration of contrast medium or exposure to
43 ionizing radiation.
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50 For evaluating coronary endothelial function, acetylcholine infusions during
51 X-ray coronary angiography or coronary flow measurement by an intracoronary
52 Doppler flow wire have been used [27]. However, the clinical utility of these methods
53 is limited to patients with a high probability of coronary artery disease due to their
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invasiveness. A noninvasive approach that permits assessment of coronary
endothelial function is desirable. Several investigators have used myocardial
perfusion positron emission tomography (PET) to assess MBF before and during the
CPT [24-25, 28-30]. One previous PET study demonstrated that cigarette smoking
causes impairment of endothelium-dependent coronary vasodilatory capacity and
abnormal coronary flow response to CPT [28]. However, myocardial perfusion PET is
a more complex and time-consuming method than MRI. MRI flow measurement does
not expose patients to ionizing radiation nor does it require venous injection of
contrast medium; thus, an MR approach using a 1.5 tesla MR system can be used in
many clinical hospitals.

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In the present study, MRI measurement of MBF in non-smokers was $0.88 \pm$
 0.19 ml/min/g at rest, in good agreement with resting MBF values reported in previous
studies using myocardial perfusion PET [28-30]. A previous PET study using
 ^{15}O -water demonstrated that MBF at rest was 0.80 ± 0.14 ml/min/g in 12 young
non-smokers without coronary risk factors [29]. Another PET study using
 ^{13}N -ammonium demonstrated that MBF at rest was 0.75 ± 0.17 ml/min/g in 10 healthy
subjects without coronary risk factors [28]. In addition, MRI measurement of resting
MBF in the present study was consistent with values calculated from CS flow divided
by LV mass, a method used by Kawada et al. [18] (0.74 ± 0.23 ml/min/g) and by
Schwitter et al. [31] (0.53 ± 0.14 ml/min/g).

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Because MBF at rest and after sympathetic stimulation is strongly determined
by cardiac workload, we corrected MBF values for corresponding RPP in this study.
According to previous studies [8, 29-30, 32-34], the percent change of MBF during
CPT in healthy young non-smokers was 4.5-37% with RPP correction and 40-55%
without correction. Siegrist et al. [25] reported that the change of MBF during the CPT

1 was significantly lower after correcting by RPP. In our study, the percent change of
2 MBF during the CPT in non-smokers was approximately 30%, in concordance with
3 the results of previous studies using RPP-corrected MBF.
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7 In the current study, impairment of coronary endothelial function in young
8 healthy smokers was detected using a noninvasive PC-MRI approach. Mean Δ MBF
9 during the CPT in smokers (0.02 ± 0.20 ml/min/g) was significantly lower than in
10 non-smokers (0.26 ± 0.18 ml/min/g, $P = 0.005$). The impaired MBF response to the
11 CPT in smokers observed in the present study is in agreement with the findings of
12 previous PET studies [28-29]. Schindler et al. [28] investigated MBF response to the
13 CPT in smokers using ^{13}N -ammonium PET. They found that Δ MBF during the CPT in
14 smokers was -0.08 ± 0.16 ml/min/g. In the present study, the 95% CI of Δ MBF was
15 0.16 to 0.35 ml/min/g for non-smokers, and -0.10 to 0.14 ml/min/g for smokers,
16 indicating that an MRI approach with the CPT can detect impaired coronary
17 endothelial dysfunction in young smokers.
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33 Accuracy of phase-contrast flow volume MRI measurements in small blood
34 vessels depends on spatial resolution. A previous study demonstrated that accurate
35 blood flow volume can be determined with PC-MRI if the number of pixels per vessel
36 diameter is 3 or greater [35]. In our current study, PC-MRI was acquired with a field of
37 view of 240×194 mm, acquisition matrix of 160×112 , acquisition pixel size of $1.5 \times$
38 1.7 mm and reconstruction resolution of 0.9×0.9 mm. These parameters allowed for
39 > 3 pixels per vessel diameter. Thus, the spatial resolution in the present study was
40 acceptable for quantifying flow volume in the CS.
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53 As reviewed by Czernin and Waldherr [36], cigarette smoking acutely
54 increases coronary blood flow in healthy individuals by up to 40%. In this study, to
55 investigate the long-term effect of cigarette smoking on MBF response to CPT, all
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1 subjects abstained from smoking for at least 12 hours before MRI examination. The
2 mechanism by which smoking causes endothelial dysfunction is thought to be
3 primarily the effects of oxidant chemicals. Oxidant chemicals degrade nitric oxide and
4 reduce nitric oxide release, therefore antagonizing the actions of nitric oxide to dilate
5 blood vessels and inhibiting platelet aggregation [8]. A previous study demonstrated
6 that coronary endothelial dysfunction was reversible by short-term smoking cessation
7 in young smokers, but not in middle-aged smokers [37]. Long-term smoking exposure
8 could lead to more advanced coronary endothelial dysfunction and atherosclerosis
9 possibly via oxidative stress.
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22 Several limitations need to be acknowledged in this study. First, the number
23 of subjects was limited and a larger number of subjects might be necessary to confirm
24 our findings. However, an impaired CS flow response to the CPT in young male
25 smokers was clearly demonstrated with the phase contrast cine MRI with sufficient
26 inter- and intra-observer variability in this study. In addition, MBF at rest and during
27 the CPT as well as Δ MBF observed in this study are in good accordance with the
28 results by previous PET studies [28-30]. The current study shows that MR CPT
29 method has great potential for noninvasive assessment of coronary endothelial
30 function. Second, only male smokers and non-smokers were enrolled in the present
31 study. A recent study in young, healthy men and women demonstrated a higher
32 increase in MBF during the CPT in women than in men, presumably because
33 estrogen improves coronary endothelial function [32]. Because MBF response to CPT
34 is smaller in men, the feasibility and reproducibility of assessing Δ MBF during the
35 CPT is more difficult in men than in women. Thus, the major aims of this study, to test
36 the feasibility and reproducibility of the MR CPT method, have been validated in the
37 current study. However, further study is necessary to evaluate the effect of smoking
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1 on coronary endothelial function in women. Third, the present technique was not
2 compared with invasive measurement of CS flow, which is considered to be a gold
3 standard measurement. However, since the purpose of the present study was to
4 explore the feasibility of assessing coronary endothelial function in asymptomatic
5 volunteers, it was not considered ethically appropriate to perform intracoronary
6 catheterization or transesophageal echocardiography in the present study.
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14 In conclusion, an impaired CS flow response to the CPT in young male
15 smokers was clearly demonstrated with PC-MRI by using a 1.5 tesla MR system that
16 is widely available. This technique has sufficient inter- and intra-observer variability.
17 MRI measurement of the response to the CPT could be of great value for assessing
18 coronary endothelial dysfunction and coronary microvascular disease.
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28 **Acknowledgments** The authors would like to thank the Advanced School for Core
29 Investigators program organized by the Asian Society of Cardiovascular Imaging for
30 providing valuable suggestions and comments on our research.
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Figure Legends

Fig. 1 Coronary sinus (CS) flow measurement by phase-contrast cine MRI. **a** A representative axial cine image of the CS with slice orientation for flow imaging (*solid line*). Representative phase-contrast cine images are also depicted: **b** magnitude image and **c** velocity map of the CS (*arrows*).

Fig. 2 Representative coronary sinus (CS) volume flow curves in the cardiac cycle at baseline and during the cold pressor test (CPT). Peak volume flow in CS was observed during early diastole.

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0.10 ml/min/g and intra-observer variability was 0.02 ± 0.07 ml/min/g.

Fig. 6 Bland-Altman plots of (a) inter-observer and (b) intra-observer variability of percent change of myocardial blood flow (MBF). The mean difference in MBF inter-observer variability was $2.3 \pm 12.7\%$ and intra-observer variability was $2.6 \pm 10.5\%$.

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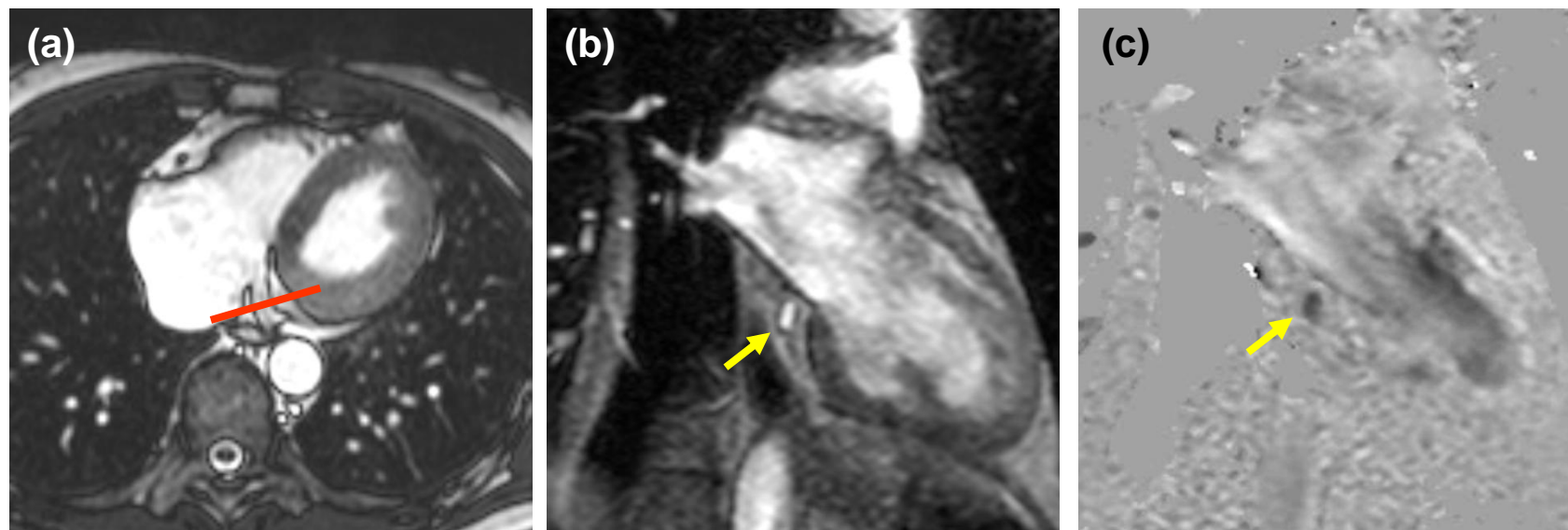


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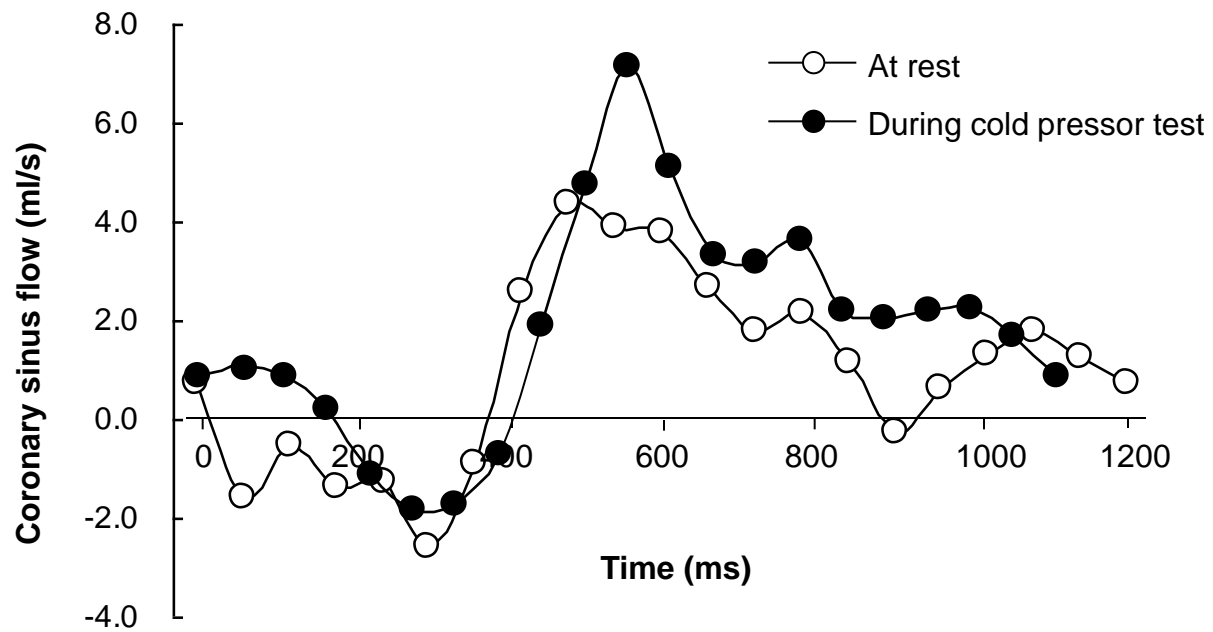


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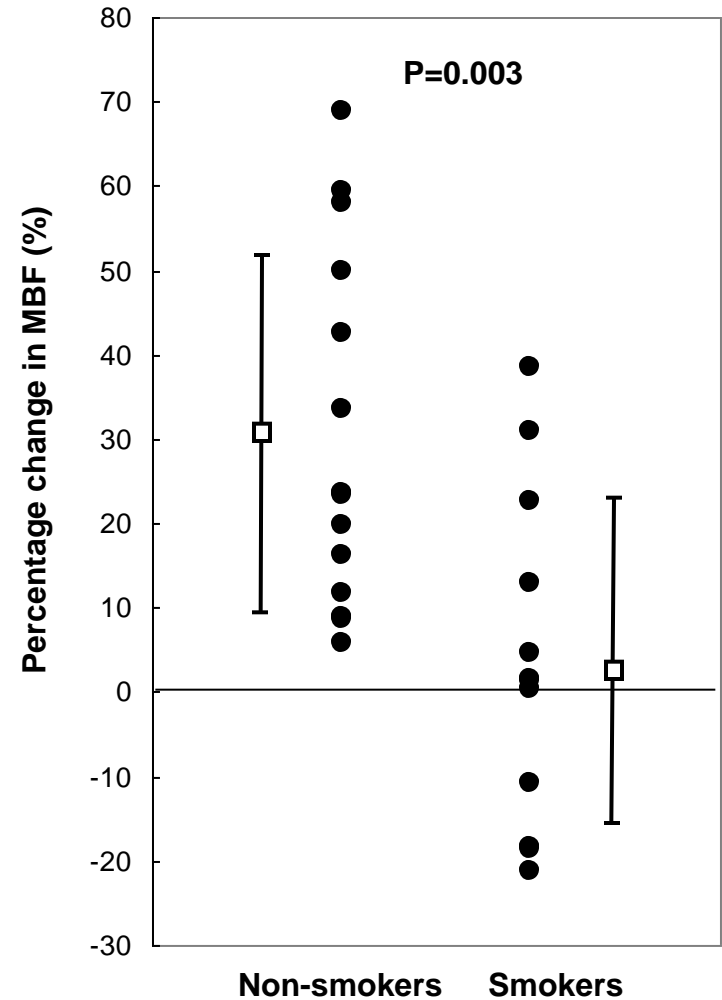
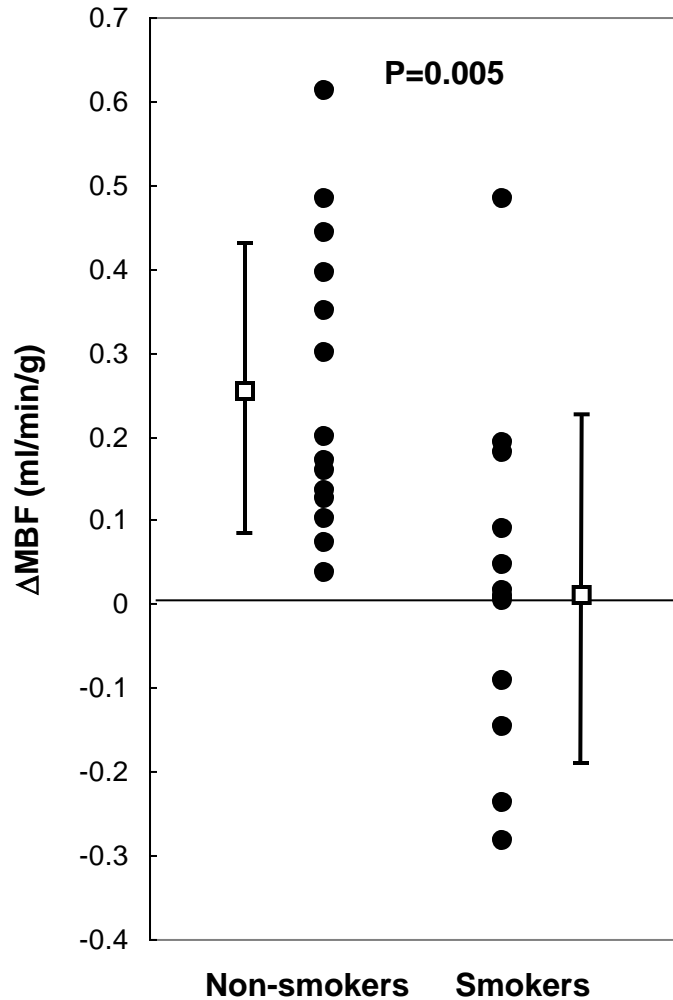


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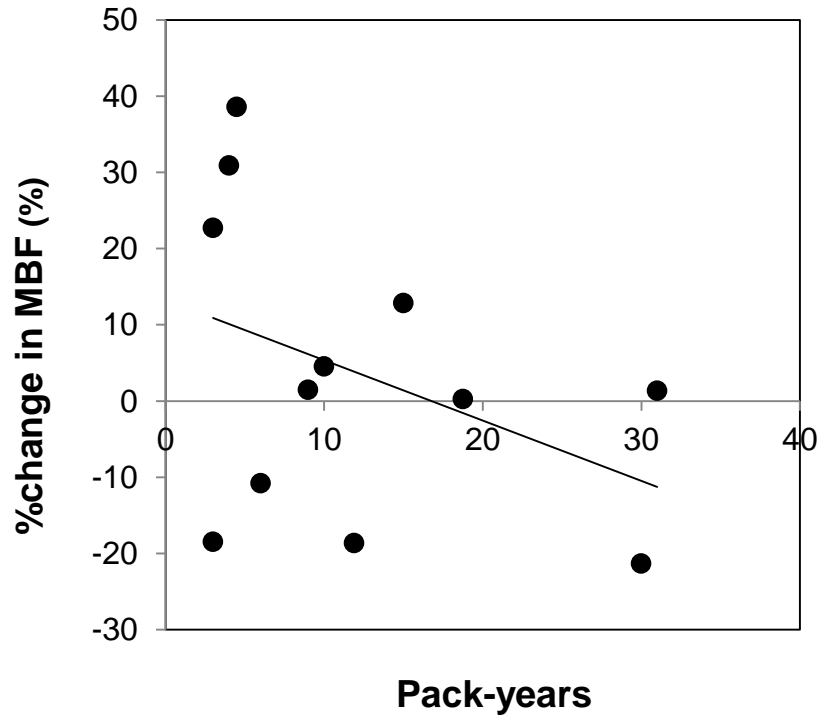


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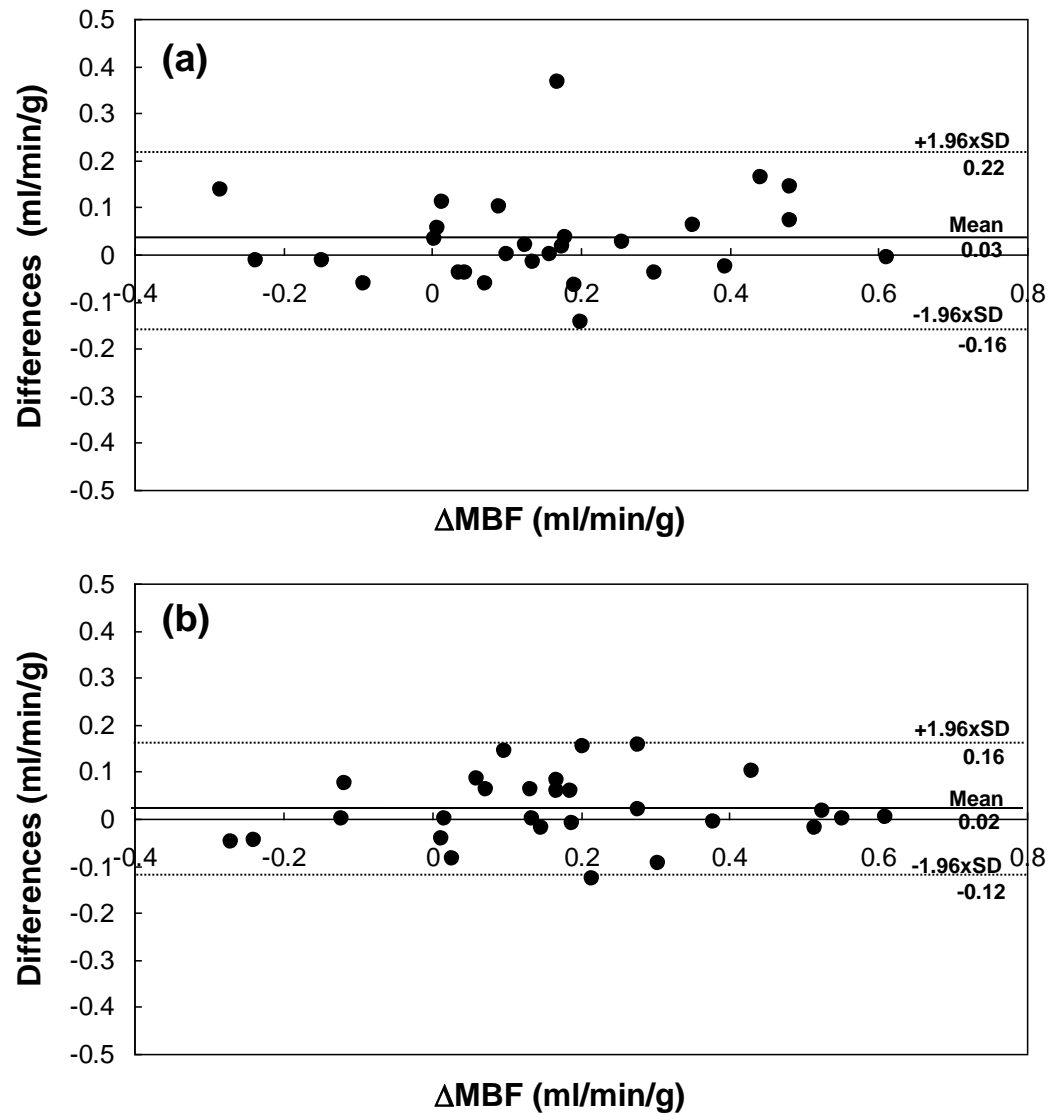


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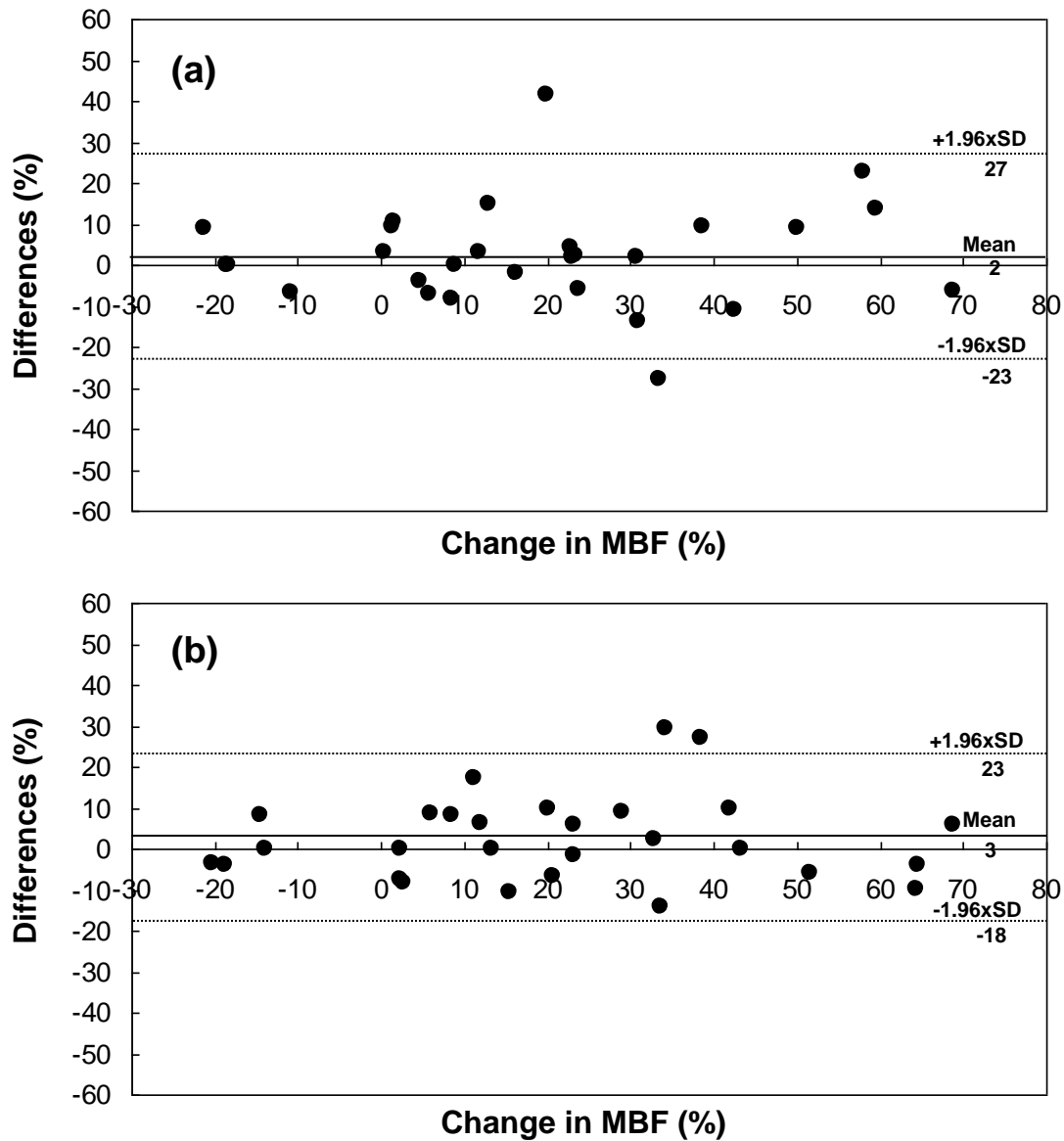


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Table 1 Clinical characteristics of subjects

Variables	Non-smokers <i>n</i> = 14	Smokers <i>n</i> = 12	<i>P</i> value
Age (years)	31 ± 6	33 ± 8	0.30
Body mass index (kg/m ²)	22 ± 2	22 ± 3	0.75
Systolic blood pressure (mmHg)	118 ± 7	123 ± 14	0.38
Diastolic blood pressure (mmHg)	63 ± 6	66 ± 7	0.27
Heart rate (beats/min)	62 ± 9	64 ± 10	0.67
Total cholesterol (mg/dl)	200 ± 34	176 ± 28	0.09
Triglycerides (mg/dl)	105 ± 51	94 ± 57	0.67
Low-density lipoprotein cholesterol (mg/dl)	121 ± 27	111 ± 19	0.4
High-density lipoprotein cholesterol (mg/dl)	59 ± 13	53 ± 16	0.35
Serum creatinine (mg/dl)	0.90 ± 0.08	0.83 ± 0.14	0.80

All results are expressed as mean ± standard deviation

Table 2 Change in hemodynamics and myocardial blood flow (MBF) values during the cold pressor test (CPT)

	Measurement	Baseline (rest)	During CPT	% Change	P value
Non-smokers <i>n</i> = 14	Systolic blood pressure (mmHg)	118 ± 7	138 ± 12	18 ± 10	<0.001
	Diastolic blood pressure (mmHg)	63 ± 6	79 ± 9	25 ± 11	<0.001
	Heart rate (beats/min)	62 ± 9	74 ± 15	19 ± 17	0.001
	RPP (mmHg/min)	Median, 7110 IQR, 1081	Median, 9697 IQR, 3637	Median, 37 IQR, 21	0.001
	MBF (ml/min/g)	0.88 ± 0.19	1.13 ± 0.26	31 ± 21	<0.001
Smokers <i>n</i> = 12	Systolic blood pressure (mmHg)	123 ± 14	147 ± 18	20 ± 12	<0.001
	Diastolic blood pressure (mmHg)	66 ± 7	83 ± 11	26 ± 13	<0.001
	Heart rate (beats/min)	64 ± 10	75 ± 21	18 ± 27	0.045
	RPP (mmHg/min)	Median, 7543 IQR, 1360	Median, 9658 IQR, 6062	Median, 33 IQR, 32	0.004
	MBF (ml/min/g)	0.94 ± 0.26	0.96 ± 0.30	4 ± 20	0.73

All results except for rate-pressure product (RPP) are expressed as mean ± standard deviation. RPP values are expressed as median and interquartile range (IQR)

Table 3 Inter- and Intra-observer variation

Inter-observer variation	Intra-class correlation coefficient	Repeatability coefficient	Mean absolute difference
MBF at rest	0.91	0.19 ml/min/g	0.07 ± 0.07 ml/min/g
MBF during the CPT	0.96	0.14 ml/min/g	0.07 ± 0.05 ml/min/g
ΔMBF	0.90	0.19 ml/min/g	0.07 ± 0.07 ml/min/g
Percentage change in MBF	0.87	25.0%	8.9 ± 9.2%

Intra-observer variation	Intra-class correlation coefficient	Repeatability coefficient	Mean absolute difference
MBF at rest	0.95	0.15 ml/min/g	0.06 ± 0.05 ml/min/g
MBF during the CPT	0.98	0.10 ml/min/g	0.04 ± 0.04 ml/min/g
ΔMBF	0.95	0.14 ml/min/g	0.06 ± 0.05 ml/min/g
Percentage change in MBF	0.91	20.5%	8.0 ± 7.1%

MBF myocardial blood flow, *CPT* cold pressor test

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JASCI-13-084

MANUSCRIPT ID NUMBER

Altered coronary endothelial function in young smokers....

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E-mail: yasutaka@clin.medic.mie-u.ac.jp

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